



## 80 kV 结合迭代算法进行多层螺旋 CT 小儿胸部成像可行性

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**【摘要】目的:**探讨多层螺旋CT(MSCT)低千伏小儿胸部成像的可行性和相关图像质量评价。**方法:**60位行低千伏胸部扫描的儿童(2个月~9岁,中位数2岁)纳入研究。使用256层CT(Philips Brilliance iCT)完成胸部平扫(80 kV, 10~15 mAs),并记录辐射剂量长度乘积(Dose Length Product, DLP),计算有效辐射剂量(Effective Dosage, ED)。所有图像数据采用6组不同的滤波函数进行回顾性重建:A组,滤波反投影(Filtered Back Projection, FBP)+平滑函数;B组,FBP+标准函数;C组,FBP+锐利函数;D组,迭代 $iDose^4$ +平滑函数;E组, $iDose^4$ +标准函数;F组, $iDose^4$ +锐利函数。在工作站上分别完成多平面投影重建(Multi-Planar Reformation, MPR)、最小密度投影(Minimum Intensity Projection, MinIP)和容积重建(Volume Rendering, VR),并在左心室最大的横断面测量脂肪、肌肉、降主动脉和肺野的图像噪声值,由两位资深放射科医师共同评价图像质量。**结果:**迭代图像质量评价优于传统滤波反投影图像,D组在降主动脉横断面上噪声和信噪比与A组相比,分别下降55%、提高69%,DLP为( $6.4\pm2.6$ ) mGy·cm,ED为( $0.11\pm0.04$ ) mSv。**结论:**80 kV结合迭代算法的低剂量MSCT小儿胸部成像是可行的。

**【关键词】**小儿胸部;辐射剂量;血管造影术;小儿体层摄影术;迭代重建;多层螺旋CT

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## Feasibility of multi-slice spiral computed tomography based on 80 kV combined with iterative algorithm for children's chest imaging

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**Abstract:** Objective To discuss on the feasibility and related image quality of multi-slice spiral computed tomography (MSCT) with low-kilovolt for children's chest imaging. Methods Sixty children, aged between 2 months to 9 years, with a median of 2 years, who received low-kilovolt chest scan, were selected. The chest plain scans of 80 kV and 10-15 mAs were carried out by using the Philips Brilliance iCT scanner of 256 slices. The dose length product (DLP) was recorded, and the effective dosage (ED) was calculated. All image data were retrospectively reconstructed by using six different filter functions, filtered back projection (FBP)+smooth function for group A, FBP+standard function for group B, FBP+sharp function for group C,  $iDose^4$ +smooth function for group D,  $iDose^4$ +standard function for group E,  $iDose^4$ +sharp function for group F. The multi-planar reformation, minimum intensity projection and volume rendering were respectively conducted on workstation. The image noise of fat, muscle, descending aorta and lung field were measured at the largest cross-section of left ventricle. The image quality was independently evaluated by 2 experienced radiologists. Results The quality evaluations of  $iDose^4$  images were significantly better than those of traditional FBP images. Compared with group A, group D reduced the noise at the cross-section of descending aorta by 55%, and increased signal-noise ratio by 69%. The DLP was ( $6.4\pm2.6$ ) mGy·cm, and ED was ( $0.11\pm0.04$ ) mSv. Conclusion The low dose MSCT based on 80 kV combined with iterative algorithm is feasible for children's chest imaging.

**Key words:** children's chest; radiation dose; angiography; tomography of children; iterative reconstruction; multi-slice spiral computed tomography

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## 前言

随着CT技术的飞速发展,通过CT检查的疾病检出率逐年提高,尤其是在肺部疾病的筛查上有着明显的优势,如肺炎、肺结节、胸腺肿瘤等普通X线检查无法捕捉到的胸部细微病变,但辐射剂量也慢慢成为不可忽视的问题。有研究表明接受过X线检查的人,当其超过75岁时,癌症发生概率将增加0.6%,主要是膀胱癌、结肠癌和白血病<sup>[1]</sup>。儿童尤其是低龄小儿对放射线的敏感性远高于成人,小儿受辐照年龄越小,致癌危险越大<sup>[2]</sup>。滤波反投影(Filtered Back Projection,FBP)作为传统的CT图像重建方法发展已经超过25年<sup>[3]</sup>,其结合电流自动调制技术<sup>[4]</sup>、降低管电压<sup>[5]</sup>、大螺距<sup>[6]</sup>等都可以应用于CT扫描来降低辐射剂量,但也受制于其算法,无法大幅度降低剂量。近年来飞速发展的迭代重建算法以大幅度降低噪声为特征已经得到广泛认可<sup>[7-9]</sup>。朱景雨等<sup>[10]</sup>同时使用低管电压和迭代重建算法,在小儿门静脉低剂量成像研究得到认可,然而在小儿头颅研究上得到的结果不甚理想。本次以小儿胸部为目标,探讨复合CT成像技术在小儿胸部中的可行性分析,以期可以常规应用于临床检查<sup>[10-11]</sup>。

## 1 材料与方法

### 1.1 一般资料

收集60例患者在本院行CT低千伏检查的患儿,男38例,女22例。年龄2个月~5岁,年龄中位数2岁,所有的患者家属都知情同意。

### 1.2 CT检查方法

采用PHILIPS Brilliance 256层ICT,探测器为128 mm×0.625;患儿采取仰卧位,于平静呼吸下进行扫描。对于不合作的患儿,待其熟睡或检查前服用10%水合氯醛0.5 mL/kg体质量镇静后进行扫描,扫描范围从肺尖到膈底。本文采用的扫描条件为80 kV、10~15 mAs、螺距0.92、准直器128 mm×0.625,球管旋转1周时间为0.4 s,层厚5 mm,间隔5 mm。分别记录每位患儿剂量长度乘积(Dose Length Product, DLP),并计算有效剂量(Effective Dosage, ED), $ED=k\times DLP$ ,小儿的胸部转换系数k采用0.026 mSv·mGy<sup>-1</sup>·cm<sup>-1</sup>(小儿<2岁)和0.018 mSv·mGy<sup>-1</sup>·cm<sup>-1</sup>(小儿>2岁)<sup>[12]</sup>。

### 1.3 图像后处理与评价

将60例患儿扫描的所有图像数据采用6组不同的滤波函数进行回顾性重建:A组,FBP+平滑函数;B

组,FBP+标准函数;C组,FBP+锐利函数;D组,迭代4(iDose<sup>4</sup>)+平滑函数;E组,iDose<sup>4</sup>+标准函数;F组,iDose<sup>4</sup>+锐利函数。重建图像数据导入PHILIPS Extended Workspace工作站,重建层厚1.0 mm,层间隔0.5 mm,重叠层厚0.5 mm,重建FOV 350 mm。在工作站上分别完成平面投影重建(Multi-Planar Reformation, MPR)、最小密度投影(Minimum Intensity Projection, MinIP)和容积重建(Volume Rendering, VR),并在左心室最大的横断面测量脂肪、肌肉、降主动脉和肺野的兴趣区(ROI)的CT值及其图像噪声(SD)值,并计算各组织的信噪比(Signal-to-Noise Ratio, SNR)。SNR运算公式为: $SNR=ROI_T/SD_T$ ,T代表不同组织<sup>[13]</sup>。由两位资深放射科医生对图像质量共同评价,用4分评定法:4分,图像无伪影,噪声很轻;3分,图像略有噪声和伪影,但不影响临床诊断;2分,图像有一定的噪声和伪影,仍能满足临床诊断;1分,图像噪声伪影较大,无法满足诊断要求。

### 1.4 统计学分析

采用SPSS19.0统计学软件进行分析,计量资料采用均数±标准差表示。对6组图像的SD值、SNR值和重建图像(MPR,MinIP,VR)评分采用完全随机设计方差分析法(One-Way ANOVA),组间比较采用LSD法。并对两位医师的评价一致性进行Kappa检验。以P<0.05作为差异有显著意义的检验标准。

## 2 结果

### 2.1 横断面测量客观比较

6组图像横断面胸部各个组织的图像SD值和SNR值见表1。各组间的SD和SNR值均有显著性差异(P<0.01),以A组与D组的降主动脉SD值和SNR值比较为例,D组iDose<sup>4</sup>+平滑函数的图像重建模式比A组FBP+平滑函数SD值下降约55%,SNR值提高约69%。

### 2.2 MPR、MinIP和VR图像评价

6组重建图像组间评价比较均有显著性差异(P<0.05)。以D、E两组各项评分最高,图像质量优秀;C组与F组评分较低,即C组与F组图像的噪声和伪影较大,不一定能满足临床诊断要求。两名医师图像评分一致性较好(Kappa=0.827,P<0.05)。见表2。

基于iDose<sup>4</sup>迭代算法的图像质量明显高于传统FBP重建的图像,三维重建图像上可以明显发现迭代算法使用相同滤过函数,与FBP图像相比,图像噪声明显降低,图像信噪比大幅度提高。见图1~3。

表1 6组胸部图像各组织CT测量值( $\bar{x} \pm s$ )  
Tab.1 CT values of tissues in 6 groups of chest images (Mean $\pm$ SD)

Group	SD value				SNR value			
	Fat	Muscle	Descending aorta	Lung field	Fat	Muscle	Descending aorta	Lung field
A	31.30 $\pm$ 12.58	54.23 $\pm$ 27.01	48.75 $\pm$ 29.85	39.09 $\pm$ 14.27	4.39 $\pm$ 1.74	1.47 $\pm$ 0.81	1.08 $\pm$ 0.74	20.33 $\pm$ 7.06
B	42.57 $\pm$ 4.37	85.47 $\pm$ 25.52	78.43 $\pm$ 22.78	39.17 $\pm$ 10.95	3.08 $\pm$ 0.54	0.77 $\pm$ 0.05	1.06 $\pm$ 0.44	17.79 $\pm$ 3.35
C	168.41 $\pm$ 7.41	366.33 $\pm$ 28.03	365.03 $\pm$ 114.56	194.33 $\pm$ 66.71	0.35 $\pm$ 0.03	0.21 $\pm$ 0.13	0.31 $\pm$ 0.17	3.84 $\pm$ 1.73
D	16.29 $\pm$ 7.13	24.89 $\pm$ 10.29	21.87 $\pm$ 11.02	19.16 $\pm$ 7.83	8.83 $\pm$ 4.13	3.91 $\pm$ 1.33	3.44 $\pm$ 1.59	37.98 $\pm$ 20.87
E	21.01 $\pm$ 8.48	32.58 $\pm$ 12.94	29.23 $\pm$ 14.34	25.33 $\pm$ 8.79	6.71 $\pm$ 2.57	3.23 $\pm$ 1.07	2.76 $\pm$ 1.13	31.21 $\pm$ 11.21
F	215.02	191.50 $\pm$ 9.84	205.06 $\pm$ 60.06	147.10 $\pm$ 21.51	6.71 $\pm$ 2.57	0.44 $\pm$ 0.21	0.49 $\pm$ 0.24	4.76 $\pm$ 1.34
P value	<0.01	<0.01	<0.01	<0.01	<0.01	<0.01	<0.01	<0.01
F value	189.76	215.02	194.94	104.17	12.31	9.67	5.48	8.44

filtered back projection (FBP)+smooth function for group A, FBP+standard function for group B, FBP+sharp function for group C, iDose<sup>4</sup>+smooth function for group D, iDose<sup>4</sup>+standard function for group E, iDose<sup>4</sup>+sharp function for group F.

One-way analysis of variance, also named F test, is used for testing the significance of mean difference of more than 2 samples, the comprehensive comparison among groups. The larger the F value is, the more obvious the significant difference is.

SD: Standard deviation; SNR: Signal-noise ratio

表2 6组MPR、MinIP和VR图像评价( $\bar{x} \pm s$ )Tab.2 Image evaluation of MPR, MinIP and VR in six groups (Mean $\pm$ SD)

Group	MPR	MinIP	VR
A	2.46 $\pm$ 0.51	2.75 $\pm$ 0.52	2.68 $\pm$ 0.55
B	2.33 $\pm$ 0.58	2.67 $\pm$ 0.58	2.14 $\pm$ 0.38
C	1.33 $\pm$ 0.47	1.68 $\pm$ 0.72	1.29 $\pm$ 0.49
D	3.71 $\pm$ 0.46	3.93 $\pm$ 0.26	3.86 $\pm$ 0.36
E	3.07 $\pm$ 0.47	3.43 $\pm$ 0.51	3.39 $\pm$ 0.49
F	1.67 $\pm$ 0.63	2.54 $\pm$ 0.38	2.04 $\pm$ 0.68
P value	<0.05	<0.01	<0.01
F value	31.59	6.37	49.68

MPR: Multi-planar reformation; MinIP: Minimum intensity projection; VR: Volume rendering

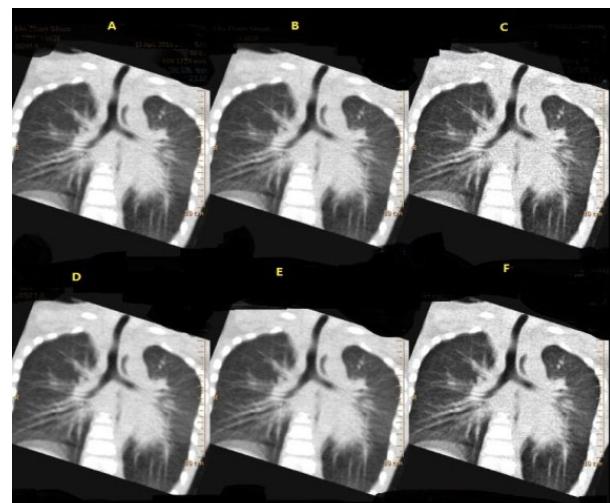


图2 肺窗冠状位MinIP图

Fig.2 Coronary MinIP with lung window

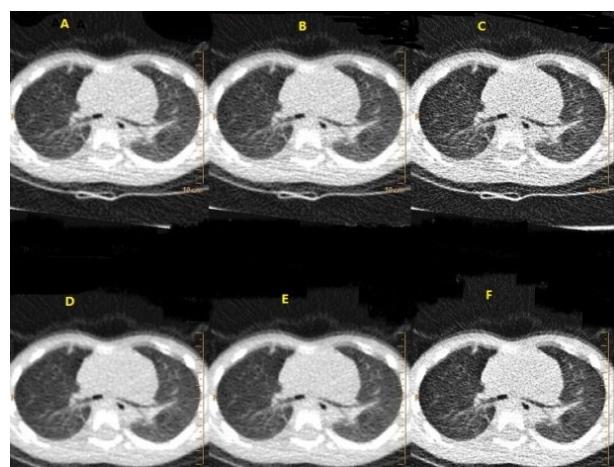


图1 肺窗MPR横断面图

Fig.1 Cross-section of MPR with lung window

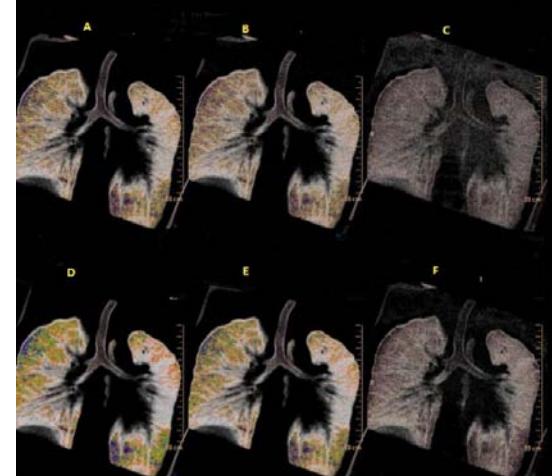


图3 肺窗冠状位VR图

Fig.3 Coronary VR with lung window



图1~3编号的A~F分别代表A~F组重建图像。图1由迭代重建的D组和E组MPR图像伪影和噪声明显优于FBP重建的A组和B组,滤过函数为Sharp的C组和F组噪声明显增大,但图像对比度和图像边缘锐利度明显提高,F组图像噪声明显小于C组。图2中6组图像的MinIP图像均能较好地显示气道和支气管分支,对于气道异物的筛查都能很好地满足临床诊断,D~F组图像信噪比明显优于A~C组。图3中6组VR重建图像都能较好地显示支气管与周围组织的空间位置关系,D组和E组图像更优,但6组图像均能满足临床诊断。

### 2.3 辐射剂量测量

本次研究所记录的总体辐射DLP为( $6.4 \pm 2.6$ ) Gy·cm,总体ED为( $0.11 \pm 0.04$ ) mSv,相当于几张成人胸片的剂量0.02 mSv,具有很大的临床应用价值。

## 3 讨论与结论

小儿低剂量CT扫描技术的使用应该遵循最优化原则,即满足临床诊断要求的基础上,尽可能地降低患儿的辐射剂量。降低管电压可以大幅度降低辐射剂量,同时可以增加图像对比度,但是会大大增加图像噪声。低剂量扫描在传统的FBP重建模式下,会大大增加图像噪声,CT图像重建的实质是按照采集后的数据,求解图像矩阵中像素,随后重新构造图像的过程,FBP的特点是先在连续域解析处理,最后离散化以利用计算机计算。FBP是基于解析求反公式的闭合形式,要求投影数据是精确完整的,实际上无法实现<sup>[4,14]</sup>。iDose<sup>4</sup>迭代技术可以在FBP重建的基础上降低图像的噪声,提高扫描图像质量,所以合理应用iDose<sup>4</sup>重建技术可以抑制重建图像噪声上升和图像质量的下降,达到还原图像来保证图像质量的目的。

80 kV结合迭代算法的复合成像模式在大幅度降低噪声的同时,与FBP重建图像相比,SNR有很大的提高,辐射剂量大大降低,重建图像均能满足临床诊断要求。尽管低千伏成像会导致横断面图像噪声增大,明显影响图像质量,但三维重建本身有很好的降噪作用,本方案的数据在三维重建的降噪范围内,所以最终的MinIP和VR图像仍显示优良<sup>[15]</sup>。

小儿较成人体层薄,更适合低剂量的复合成像方案,因此小儿低剂量CT检查可以具有普遍性和广泛性。本研究数据显示基于迭代算法的小儿低剂量CT胸部成像切实可行,能更好地为临床诊断和治疗提供依据。

## 【参考文献】

- [1] GONZALEZ A B, DARBY S. Risk of cancer from diagnostic X-rays: estimates for the UK and 14 other countries [J]. Lancet, 2004, 363: 345-351.
- [2] DAVID J E, CARL D E, ERIC J H, et al. Estimated risks of radiation induced fatal cancer from pediatric CT [J]. Am J Roentgenol, 2001, 176: 289-296.
- [3] FELDKAMP L A, DAVIS L C, KRESS J. Practical cone-beam algorithm [J]. J Opt Soc Am, 1984, 1(6): 612-619.
- [4] KALRA M K, MAHER M M, TOTH T L, et al. Strategies for CT radiation dose optimization [J]. Radiology, 2004, 230: 619-628.
- [5] HEYER C M, MOHR P S, LEMBURG S P, et al. Image quality and radiation exposure at pulmonary CT angiography with 100- or 120-kVp protocol: prospective randomized study [J]. Radiology, 2007, 245: 577-583.
- [6] DIEL J, PERLMUTTER S, VENKATARAMAN N, et al. Unenhanced helical CT using increased pitch for suspected renal colic: an effective technique for radiation dose reduction? [J]. Comput Assist Tomogr, 2000, 24: 795-801.
- [7] HARA A K, PADEN R G, SLIVA A C, et al. Iterative reconstruction technique for reducing body radiation dose at CT: feasibility study [J]. Am J Roentgenol, 2009, 193(3): 764-771.
- [8] PRAKASH P, KALRA M K, KAMBADAKONE A K, et al. Reducing abdominal CT radiation dose with adaptive statistical iterative reconstruction technique [J]. Invest Radiol, 2010, 45(4): 202-210.
- [9] MARIN D, NELSON R C, SCHINDERA S T, et al. Low-tube-voltage, high-tube-current multidetector abdominal CT: improved image quality and decreased radiation dose with adaptive statistical iterative reconstruction algorithm-initial clinical experience [J]. Radiology, 2010, 254(1): 145-153.
- [10] 朱景雨, 李惠民, 蔡静, 等. 基于迭代算法小儿门静脉低剂量螺旋CT成像可行性[J]. 中国医学物理学杂志, 2015, 32(5): 728-732.  
ZHU J Y, LI H M, CAI J, et al. Feasibility of multi-slice computed tomography with low-dose based on iterative algorithms in children portal vein imaging [J]. Chinese Journal of Medical Physics, 2015, 32 (5): 728-732.
- [11] 朱景雨, 李惠民, 陈兆学, 等. 80kV结合迭代算法进行多层螺旋CT门静脉成像的可行性研究[J]. 中华放射医学与防护杂志, 2013, 33(5): 569-572.  
ZHU J Y, LI H M, CHEN Z X, et al. Feasibility of MSCT portal vein imaging with 80 kV combined iterative method [J]. Chinese Journal of Radiological Medicine and Protection, 2013, 33(5): 569-572.
- [12] JESSEN K A, BONGARTZ G, GELEIJNS J, et al. European Guidelines on quality criteria for computed tomography [M]. Luxembourg: European Commission, 2000: 16262.
- [13] 杜煜, 时高峰, 王亚宁. 双源头颅CTA低千伏扫描的初步研究[J]. 实用医学杂志, 2013, 29(12): 1930-1933.  
DU Y, SHI G F, WANG Y N. Preliminary study on dual head CTA low kV scanning [J]. The Journal of Practical Medicine, 2013, 29 (12): 1930-1933.
- [14] FUNAMA Y, AWAI K, NAKAYAMA Y, et al. Radiation dose reduction without degradation of low-contrast detectability at abdominal multisecti on CT with a low-tube voltage technique: phantom study [J]. Radiology, 2000, 237: 905-910.
- [15] 朱景雨, 李惠民, 蔡静, 等. 256层CT支气管动脉成像技术优化[J]. 中国医学计算机成像杂志, 2014, 20(6): 561-564.  
ZHU J Y, LI H M, CAI J, et al. Optimization of CT angiography technique of bronchial artery with 256-slice MSCT [J]. Chinese Computed Medical Imaging, 2014, 20(6): 561-564.